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5  
6 *This manuscript was published as formal in:*

7 *CARBOHYDRATE POLYMERS Volume: 170 Pages: 60-71 Published: AUG 15*  
8 *2017*

9 <https://doi.org/10.1016/j.carbpol.2017.04.055>

10 <https://www.sciencedirect.com/science/article/pii/S014486171730454X>



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14 **Title:**

15 **Development of Biocompatible Glycodynameric Hydrogels Joining two Natural Motifs**  
16 **by Dynamic Constitutional Chemistry**

17 *by:*

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## 30 **ABSTRACT**

31 The paper focusses on the synthesis of novel hydrogels by joining natural biodegradable  
32 compounds with the aim to achieve biocompatible materials for bio related applications. The  
33 hydrogels were prepared from chitosan and citral by constitutional dynamic chemistry,  
34 incorporating both molecular and supramolecular dynamic features. The hydrophobic flexible  
35 citral has been reversible immobilized onto the hydrophilic chitosan backbone *via* imine  
36 bonds to form amphiphilic glycodynamers, which further self-ordered through supramolecular  
37 interactions into a 3D-network of biodynameric hydrogel. The synthetic pathway has been  
38 demonstrated by NMR and FTIR spectroscopy, X-ray diffraction and polarized light  
39 microscopy. Studies of the hydrogel morphology revealed a 3D porous microstructure, whose  
40 pores size correlated with the crosslinking degree. Rheological investigations evidenced high  
41 elasticity, thermo-responsiveness and thixotropic behavior. As a proof of the concept, the  
42 hydrogels proved *in vivo* biocompatibility on laboratory mice. The paper successfully  
43 implements the constitutional dynamic chemistry in generation of chitosan high performance  
44 hydrogels.

45 **KEYWORDS:** hydrogel, chitosan, dynamic constitutional chemistry, rheology,  
46 biocompatibility

47

## 48 **1. INTRODUCTION**

49 Hydrogels are a class of soft materials mainly composed of water, with modifiable  
50 structure and functions and so with a plenty of applications in important fields of the human  
51 life – as substrates for biomedical engineering and pharmacology, environmental protection,  
52 agriculture, food industry, hygiene and so on [Chawla, Srivastava, Pandey, & Chawla, 2014;  
53 Chen et al. 2016; Jayakumar et al., 2010; Jing, Wang, Yu, Amer, & Zhang, 2013; Kamata, Li,  
54 Chung, & Sakai, 2015; Sharma et al., 2014]. Among hydrogels, those prepared from natural  
55 polymers present the advantage of bioactivity, biocompatibility and biodegradability, being  
56 especially studied for bio-related applications. In particular, chitosan-based hydrogels have  
57 the highest *in vivo* applicability due to the intrinsic properties of chitosan, such as  
58 biocompatibility and biodegradability, hemostatic, hypolipidemic, hypoglycemic, antitumoral,  
59 antimicrobial and fungicidal activity – to mention only some [Jayakumar, Menon, Manzoor,  
60 Nair, & Tamura, 2010; Padmanabhan, & Nair, 2016]. The traditional pathways of chitosan  
61 gelling use either physical crosslinkers leading to hydrogels with weak mechanical properties  
62 and uncontrolled dissolution, or chemical crosslinkers resulting in hydrogels with better  
63 mechanical strength and the advantage of controllable morphology [Padmanabhan, & Nair,

64 2016]. Since chitosan is in fact a polyamine, the main route of its chemical crosslinking is the  
65 acid condensation reaction between its amine functional moieties and dialdehydes giving  
66 imine bonds. The most encountered crosslinking agent is glutaraldehyde, which was recently  
67 demonstrated to have a certain degree of toxicity for the human body [Beauchamp, St Clair,  
68 Fennell, Clarke, & Morgan, 1992; Berger et al., 2004], fact which turned the attention of the  
69 scientific community to more friendly crosslinkers originating from natural sources,  
70 especially targeted due to their potential to preserve the biological properties and to mimic the  
71 natural tissues [Beskardes, Demirtas, Durukan, & Gumusderelioglu, 2015; Garnicia-Palafox,  
72 & Sanchez-Arevalo, 2016; Huber et al., 2017; Mikhailov et al., 2016]. Even if so much effort  
73 has been dedicated to the obtaining of chitosan based hydrogels, less attention has been paid  
74 to the potential of the imine bonds formed on the chitosan chains. Imine bonds, also known as  
75 azomethines or Schiff bases, were extensively studied for their high thermostability,  
76 thermotropic properties, ability to act as ligand, semiconducting and luminescent properties  
77 [Kaya, & Kilavuz, 2015; Sek et al., 2012; Zabulica et al. 2013; Zabulica, Perju, Bruma, &  
78 Marin, 2014; Zaltariov et al., 2015]. In addition to the above mentioned properties, lately, the  
79 reversibility of the imine bonds proved to be the most important tool in (i) dynamic covalent  
80 chemistry conferring advantageous proof reading and error checking capabilities toward  
81 supramolecular entities [Chen et al., 2013; Chen et al., 2013; Liu, & Li, 2013; Liu, Lehn &  
82 Hirsh, 2016; Roy, Bruchmannb, & Lehn, 2015; Schneider, Siegfried Hauswald, Stoll, &  
83 Mastalerz, 2012] and (ii) dynamic combinatorial chemistry toward constitutional libraries  
84 whose constituents can exchange under the pressure of external factors generating adaptive  
85 chemical systems [Clima, Peptanariu, Pinteala, Salic, & Barboiu, 2015; Hu, Zhang, &  
86 Ramström, 2015; Marin et al. 2016; Sreenivasachary, & Lehn, 2005; Zhang, & Barboiu,  
87 2016]. By dynamic covalent chemistry, challenging supramolecular architectures have been  
88 created, such as epitaxial crystals [Chen et al. 2013], microtubes [Chen et al., 2013],  
89 molecular cages, porous organic amorphous or crystalline materials [Schneider, Siegfried  
90 Hauswald, Stoll, & Mastalerz, 2012], self-healing films [Roy, Bruchmannb, & Lehn, 2015]  
91 and hydrogels [Chang, Wang, Li, An, & Qin, 2016]. Moreover, it was demonstrated that the  
92 imine linkage has the potential to drive a gelation process selecting an organogelator from a  
93 library, and plays a key role in gelling process due to its conjugation which favors the  
94 assembly of the gelator network [Sreenivasachary, & Lehn, 2005].

95         Recent and challenging studies in the area of hydrogels revealed that the obtaining of  
96 hydrogels using multi-valence binders led to superior mechanical strength and substantial  
97 elastic response of such systems which are mostly composed of water [Wang et al., 2010].

98 Outstanding, controllable mechanical properties were reached also for hydrogels with layered  
99 morphology induced by the use of metallic nanosheets [Liu et al., 2013].

100 Here we present a new approach for the preparation of hydrogels using the citral  
101 monoaldehyde as chitosan gelator, based on dynamic imine chemistry. Citral is a natural,  
102 relatively long chain, aliphatic monoaldehyde found in the oil of several plants, with lack of  
103 toxicity to the human body (LD<sub>50</sub> values more than 1000 mg/Kg), rapidly metabolized and  
104 excreted as metabolites [SIDS, 2001], increasing the potential of its use in preparation of new  
105 biocompatible and biodegradable materials. Detailed characterization studies demonstrated  
106 that the unusual gelation of chitosan in the presence of citral was driven by the competition  
107 between the imine formation and its aliphatic side chains self-organization into  
108 supramolecular layered architectures. Thus, ordered entities were obtained which in turn  
109 played the role of multi-binder crosslinkers of chitosan chains giving raise to hydrogels with  
110 remarkable mechanical properties.

111

## 112 **2. EXPERIMENTAL SECTION**

### 113 **2.1. Materials**

114 Citral (95%), low molecular weight chitosan (263 kDa, DA: 83%), D-glucosamine  
115 hydrochloride and phosphate buffer solution have been purchased from Aldrich and used as  
116 received. Acetate buffer (pH=4) was prepared in our laboratory [Iftime, Morariu, & Marin,  
117 2017].

### 118 **2.2. Synthesis of the model compound**

119 The model compound has been synthesised according to a published procedure [Safoura  
120 et al., 2014], slightly modified taking into consideration the properties of citral, as follows:  
121 100 mg D-glucosamine hydrochloride (0.463 mmol) have been solubilized in 1.4 mL  
122 methanol and mixed under vigorous stirring with a stoichiometric amount of sodium  
123 hydroxide (0.018 g; 0.463 mmol), with the purpose to obtain the free amine. After five  
124 minutes, the mixture has been filtered to remove the resulted salt. To the clear solution of the  
125 free glucosamine, 0.074 g (0.463 mmol) of citral have been added, at 35 °C, and kept under  
126 magnetically stirring about five minutes, when a white precipitate formed. The precipitate was  
127 filtered, washed three times with cold dichloromethane and dried under vacuum for 24 hours.  
128 <sup>1</sup>H NMR (DMSO-*d*<sub>6</sub>, 400 MHz) δ(ppm): 8.07, 8.05, 8.04, 8.02 (d, 1H, H<sub>b</sub>); 6.45 (s, 1H, OH  
129 from sugar unit), 5.88, 5.86 (d, 1H, OH from sugar unit), 5.1 (m, 1H, H<sub>c</sub>), 4.99 (s, 1H, OH  
130 from sugar unit), 4.78 (m, 1H, OH from sugar unit), 4.58 (m, 2H, H<sub>o</sub>), 3.71 (d, 1H, H<sub>g</sub>), 3.17,

131 3.15 (superposed peaks, 2H, H<sub>k</sub>, H<sub>j</sub>); 3.48 (superposed peaks, 1H, H<sub>n</sub>); 2.64, 2.31 (m, 2H,  
 132 H<sub>e</sub>); 2.13 (superposed peaks, 3H, H<sub>f</sub>); 1.9, 1.85 (s, 2H, H<sub>d</sub>); 1.66 (s, 3H, H<sub>b</sub>); 1.59 (s, 3H, H<sub>a</sub>).  
 133 FT-IR (ATR, cm<sup>-1</sup>): 3424 (ν<sub>OH</sub>); 2904, 2839 (ν<sub>CH<sub>2</sub></sub>, ν<sub>OH</sub>); 1644 (ν<sub>CH=N</sub>); 1618 (ν<sub>C=C</sub>); 1441,  
 134 1381 (ν<sub>C-H</sub>); 1083 (ν<sub>C-O-C</sub> pyranose); 897 (δ<sub>C-H</sub>).

### 135 2.3. Preparation of hydrogels and xerogels

136 Firstly, solutions of the two reagents were prepared by dissolving chitosan (0.06 g, 0.29  
 137 mmoles of glucosamine repeating units) in 0.7% acetic acid aqueous solution (3 mL) to give a  
 138 2% solution, and by dissolving different amounts of citral in alcohol to give a 1% solution  
 139 (Table 1). The amount of chitosan has been kept constant while the amount of aldehyde was  
 140 varied, in order to obtain hydrogels with different crosslinking degrees labelled as in Table 1.  
 141 Then, the citral solution has been added drop wise to the chitosan one, under continuous  
 142 magnetic stirring at 55 °C up to the visual examination revealed the transformation of the  
 143 pallor solution into a transparent yellowish semisolid, without air bubbles or other  
 144 macroscopic particles. In the case of the sample **C1** the gelation occurred immediately after  
 145 the entire amount of citral was added, while in the case of **C2**, a semisolid hydrogel was  
 146 obtained after 3 hours. For the other samples, hydrogels were obtained only after 24 hours.  
 147 The sample **C4.5** remained as a highly viscous liquid even after 24 hours. All hydrogels were  
 148 kept uncovered until they reached the same level as the initial solution of chitosan, indicating  
 149 the removal of ethanol. The hydrogels were kept covered another ten days to reach the  
 150 equilibrium of the imination reaction (according to the NMR experiments), and then sent to  
 151 experimental characterization. Corresponding xerogels were obtained by lyophilisation. By  
 152 weighing the precursor reagents and the xerogels it was found that no reagents were removed  
 153 during lyophilization (Table 1).

154

155 **Table 1.** The codes and the corresponding NH<sub>2</sub>/CHO molar ratio of the hydrogels

Code	C0	C1	C2	C2.5	C3	C3.5	C4	C4.5
<b>NH<sub>2</sub>:CHO ratio</b>	1:0	1:1	2:1	2.5:1	3:1	3.5:1	4:1	4.5:1
<b>mg/mmol of chitosan</b>	60/0.29	60/0.29	60/0.29	60/0.29	60/0.29	60/0.29	60/0.29	60/0.29
<b>mg/mmol of citral</b>	0	46/0.29	23/0.145	18/0.116	15/0.096	13/0.082	11.6/0.0725	10/0.064
<b>mg of xerogel</b>	60	106	83	78	75	73	71.6	70
<b>Gelation time</b>	-	3 min	3 hours	24 hours	24 hours	24 hours	24 hours	-

156

### 157 2.4. Methods

158 Nuclear magnetic resonance (NMR) spectra of the model compound and hydrogels were  
 159 recorded in deuterium oxide using a Bruker Avance DRX 400 MHz Spectrometer equipped  
 160 with a 5 mm QNP direct detection probe and z-gradients. The chemical shifts are reported as

161  $\delta$  values (ppm) relative to the residual peak of the solvent. NMR spectra were registered at  
162 each three days to establish the stabilization of the imination equilibrium. All-spectra have  
163 been processed using TopSpin 1.3 software.

164 Fourier transformed infrared (FTIR) spectra of the model compound, chitosan and  
165 xerogels were measured with a FT-IR Bruker Vertex 70 Spectrofotometer, by ATR technique.  
166 All spectra have been processed using OPUS 6.5 software.

167 Wide angle X-ray diffraction (WXR) has been done on xerogel pellets, using a  
168 Bruker D8 Avance diffractometer with the Ni-filtered Cu-K $\alpha$  radiation ( $\lambda = 0.1541$  nm). The  
169 data were recorded at 36 kV and 30 mA and the results have been handled using FullProf  
170 2000 software. The diffractograms have been registered between 2-40 $^\circ$  (2 theta degrees). The  
171 xerogels pellets were obtained by pressing with a manual Hydraulic Press, at 10 N/m $^2$ .

172 Polarized light microscopy observations were performed on thin slices of hydrogel  
173 between two clean untreated glass slides, using an Olympus BH-2 polarized light microscope.

174 The microstructure of the hydrogels has been characterized by surface and cross-  
175 section viewing with a field emission Scanning Electron Microscope SEM EDAX – Quanta  
176 200, operated at 12.5 or 20 keV accelerating voltage. The images have been handled using  
177 Image J Software in order to determine the pore size and the thickness of the pore walls.  
178 Resulted data were used to build the histograms and to determine the standard deviation  
179 values in Origin Software.

180 The gelation time has been determined as the period of time after which the reaction  
181 mixture has been visually transformed from a viscous liquid into an elastic quasi solid state.

182 The swelling measurements have been performed on square-shape pieces of xerogels  
183 which were kept in the oven over night. The measurements were performed in triplicate, using  
184 always the same amount of water or buffer solution (20 mL). By weighing the mass of the  
185 samples before and after swelling, the mass equilibrium swelling (MES) has been calculated  
186 using the equation:  $MES = (M_s - M_d) / M_d$ , where  $M_s$  is the mass of the hydrogel in swollen  
187 state and  $M_d$  the mass of the hydrogel in dried state.

188 The rheological parameters were determined using a Bohlin CVO rheometer with  
189 parallel plate geometry (60 mm diameter) and thermal control by the Peltier effect in closed  
190 system. The frequency sweep experiments were carried out at 20  $^\circ$ C and 37  $^\circ$ C, respectively,  
191 within the linear viscoelastic regime. The amplitude sweep tests have shown an extended  
192 linear viscoelastic domain corresponding to structured samples [Morariu, Bercea, & Brunchi,  
193 2015]. The oscillatory and continuous shear measurements were performed in the frequencies

194 range of 0.5 – 100 rad·s<sup>-1</sup> and in the range of shear rate ( $\dot{\gamma}$ ) from 6 x 10<sup>-2</sup> s<sup>-1</sup> to 10<sup>2</sup> s<sup>-1</sup>. From  
195 the oscillatory deformation tests, the loss modulus ( $G''$ ), the storage modulus ( $G'$ ), the  
196 complex viscosity ( $\eta^*$ ) and the loss tangent ( $\tan \delta$ ) defined as  $G''/G'$  were determined. In  
197 addition, the flow tests were performed at 20 °C in order to obtain the hysteresis loops by  
198 increasing the shear rate up to 400 s<sup>-1</sup> in 500 s followed by its reduction from 400 s<sup>-1</sup> to 0 in  
199 the next 500 s. For **C1** sample, at 20 °C, some rheological measurements were not possible  
200 due to its brittleness.

201 The hydrogels were frozen in liquid nitrogen and further submitted to lyophilization  
202 using a Christ Alpha 2-4 LD plus, Freeze Dry equipment, for 24 hours at -50 °C and 0.04  
203 mbar.

204 ***In vivo biocompatibility of the hydrogels.*** The *in vivo* biocompatibility of the hydrogels was  
205 evaluated by determining the hematological, biochemical and immune system profile of  
206 animals treated with the tested substances (saline solution, **C1**, **C2**, **C3**). For these  
207 investigations were used Swiss white mice (weighing between 25-30g) with uniform  
208 distribution by gender, purchased from the bio-base of "Grigore T. Popa" University of  
209 Medicine and Pharmacy, Iași. The animals were brought one day before, and kept in standard  
210 laboratory conditions (with 21°C±2°C constant temperature, 50-70% relative humidity and an  
211 alternating lighting regime, with ratio of light/darkness = 12 hours/12 hours), with food and  
212 water available *ad libitum*. Before the experiment, mice were placed upon a wire mesh, in a  
213 plastic box and left for two hours to acclimatize to the laboratory environment. In order to  
214 avoid the chrono-biological influences, the tests were carried out in the interval between 8-12  
215 a.m. For biocompatibility estimation, 4 groups of 6 animals each were treated  
216 intraperitoneally (i.p.) as follows: **Group 1** (coded **Control**): saline solution 0,1 mL/10g body  
217 weight - control; **Group 2** (coded **C1**): hydrogel **C1**; **Group 3** (coded **C2**): hydrogel **C2**;  
218 **Group 4** (coded **C3**): hydrogel **C3**. After 24 hours and 14 days from the intraperitoneally  
219 administration of investigated substances, the animals were anaesthetized with ethyl ether and  
220 the blood was collected from the retro orbital plexus to assess (i) the hematologic profile: - the  
221 values of erythrocytes (ER), hemoglobin (Hb), hematocrit (Ht); - the white blood cell  
222 differential: polymorphonuclear neutrophils (PMN), lymphocytes (Ly), eosinophils (E),  
223 monocytes (M), basophils (B); (ii) the liver enzymes activity: - the alanine aminotransferase,  
224 also called the glutamate pyruvate transaminase (GPT); - the aspartate aminotransferase, also  
225 called glutamic oxaloacetic transaminase (GOT); - the lactic dehydrogenase (LDH); (iii) the  
226 levels of some immune system parameters: - the phagocytic capacity of neutrophils in the

227 peripheral blood (PC); - the serum opsonic capacity (OC); - the phagocytic and bactericidal  
228 capacity of peritoneal macrophages (BC).

229 For biochemical analysis, 0.3 ml of venous blood has been drawn from the retro  
230 orbital plexus after topical anesthesia. Blood samples were collected in heparinized tubes and  
231 kept in an ice-water mixture until the moment of determination. Laboratory tests were  
232 performed using the special Analyzers for each investigated parameters [De Jong, Carraway,  
233 & Geertsma, 2012; Limon-Pacheco, & Gonsebatt, 2009; Wolf, & Andwraon, 2012].

234 On the 14<sup>th</sup> day of the experiment the serum opsonic capacity (OC) was evaluated by  
235 using the cultures of *Staphylococcus aureus 94*.

236 At the end of the experiment, the animals were euthanized under ethyl ether anesthesia  
237 and the peritoneal macrophages were removed from the intact peritoneal cavity with 10 ml  
238 HANKS solution (thermostated at 37<sup>0</sup>C). The samples were centrifugated at 1000 rpm for  
239 10 minutes, brought into contact with *Staphylococcus aureus 94* cultures, incubated for 48  
240 hours at 37<sup>0</sup>C and re-inseminated on culture media. The following immune parameters  
241 activity: phagocytic capacity (PC) and bactericidal capacity (BC) of peritoneal macrophages  
242 was investigated.

243 All the data were centralized and statistically analyzed using Student's t-Test in  
244 EXCEL program for Windows 10. Results were expressed as mean values  $\pm$  standard  
245 deviation of the mean for 6 animals in a group. The p values less than 0.05 were considered to  
246 be statistically significant comparative to those of the control group.

247 The liver fragments were collected for histopathological examination. Tissue  
248 fragments were fixed in 10% formalin, embedded in paraffin and hematoxylin&eosin (H&E)  
249 stained. The samples were examined and visualized using an optical microscope equipped  
250 with a digital system for images acquisition.

251 The experiments were performed according to the recommendations of the “Grigore  
252 T. Popa” University Committee for Research and Ethical Issues in compliance with the  
253 international regulations regarding the handling of the laboratory animals. Particularly, the  
254 duration of the experiments was the shortest possible and the number of animals used in has  
255 been reduced to the minimum sufficient to achieve adequate statistical processing of the  
256 obtained data. For ethical reasons all animals used in study have been sacrificed at the end of  
257 the experiments.<sup>11</sup>

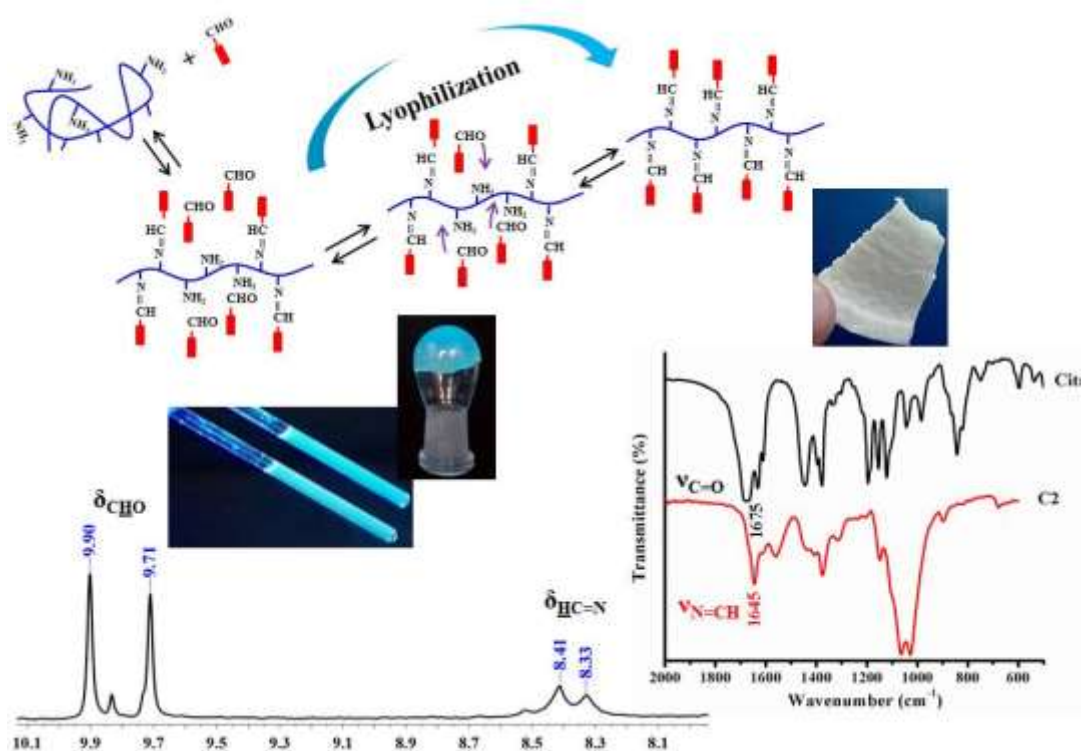
258

### 259 **3. RESULTS AND DISCUSSIONS**



260 A series of hydrogels has been obtained by reacting chitosan with citral in various  
261 molar ratios of the functional groups. The obtained hydrogels were transparent, yellowish  
262 under normal light and emitted blue light by illumination with an UV lamp (Scheme 1). The  
263 hydrogels will be referred to by the letter **C** followed by the number representing the molar  
264 ratio between the amine groups on chitosan and aldehyde functionality of citral, e.g. the  
265 hydrogel with a  $\text{NH}_2/\text{CHO}$  molar ratio of 2/1 was noted **C2**.

266 The crosslinking of chitosan with citral mono-aldehyde is an unprecedented pathway  
267 of hydrogel preparation which requires a detailed structural characterization in order to  
268 understand the driving forces governing the gelling process. To reach this goal a model  
269 compound (**MC**) was synthesized from glucosamine (the repeating unit of chitosan) and citral  
270 and analyzed as a reference. The main chemical reaction most likely to take place between the  
271 polyamine-like chitosan and citral is the acid condensation of the amino group and the  
272 electrophile carbonyl to give the imine linkage. On the other hand, it must be considered that  
273 the formation of imine in water is a reversible reaction which allows imination and trans-  
274 imination processes under the pressure of external stimuli giving a dynamic material [Chen et  
275 al., 2013; Chen et al., 2013; Liu, & Li, 2013; Roy, Bruchmannb, & Lehn, 2015; Schneider,  
276 Siegfried Hauswald, Stoll, & Mastalerz, 2012]. To monitor the chemical and physical  
277 transformations during the chitosan gelling process in the presence of citral,  $^1\text{H-NMR}$  and  
278 FTIR spectroscopies were involved.



279 **Scheme 1.** Representation of the synthesis of the hydrogels and corresponding xerogels,  
 280 highlighting the imine formation by  $^1\text{H-NMR}$  and FTIR spectra  
 281

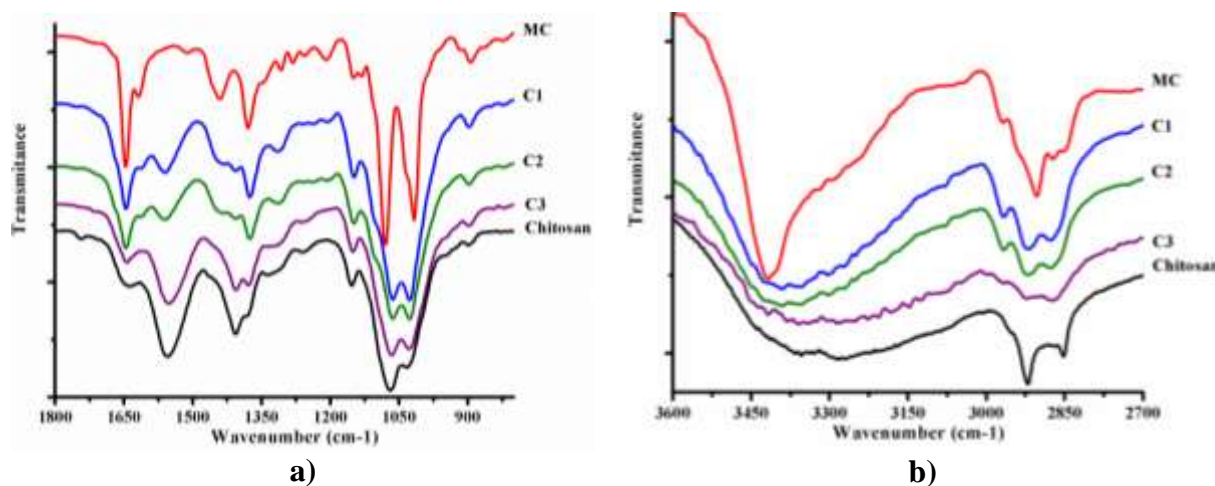
### 282 3.1. NMR characterization

283  $^1\text{H-NMR}$  evidenced the formation of the imine linkage by the presence of the specific  
 284 chemical shift of the imine proton between 8 and 9 ppm [Marin, van der Lee, Shova, Arvinte,  
 285 & Barboiu, 2015; Safoura, 2014]. The chemical shift of the imine proton in the model  
 286 compound appeared as a pair of doublets located at 8.07, 8.05 and 8.04, 8.02 ppm, due to the  
 287 *cis* and *trans* conformers (Figure S1) [Ailincai et al., 2016; Destri, Khotina, & Porzio, 1998].  
 288 The hydrogel spectra showed the chemical shift characteristic to the imine proton but also that  
 289 of the aldehyde proton indicating an equilibrium reaction (Scheme 1, Figure S2a). The signal  
 290 of the imine proton was shifted to a higher magnetic field at 8.41, 8.32 ppm, corresponding to  
 291 a deshielding effect consistent with a stronger conjugation of the newly formed imine units in  
 292 hydrogels, probably, gained due to the H-bonding and self-organization of the imine units [vu  
 293 Deb Linde, Dornseiffen, Veenland, & de Boer, 2016]. The monitoring of the evolution of the  
 294 NMR spectra over time revealed that the equilibrium position of the imine formation reaction  
 295 slowly shifted toward imine products during 10 days (Figure S2b), reaching a 1/1 molar ratio  
 296 of the newly formed imine to unreacted aldehyde (Figure S2c). This suggested the sol-gel  
 297 transition as a stimulus which favored the imine formation by imination and transimination

298 reactions, specific to the dynamic systems [Chen et al., 2013; Liu, & Li, 2013; Marin et al.,  
299 2014; Roy, Bruchmannb, & Lehn, 2015; Schneider, Siegfried Hauswald, Stoll, & Mastalerz,  
300 2012].

### 301 3.2. FTIR characterization

302 To put into evidence the chemical pathway of the hydrogel formation, FTIR spectra of  
303 the model compound and chitosan-citral xerogels were recorded. In the **MC** spectrum, the  
304 characteristic stretching vibration band of the imine group clearly appeared as a sharp peak at  
305  $1645\text{ cm}^{-1}$  in the fingerprint region, while the bands characteristic to the aldehyde ( $1675\text{ cm}^{-1}$ )  
306 and amine ( $1560\text{ cm}^{-1}$ ) groups of the reagents were missing (Figure S3). Compared to the  
307 aromatic imines, the  $-\text{CH}=\text{N}-$  band is shifted to higher wavenumbers, in agreement with the  
308 lower degree of conjugation of the imine bonding two aliphatic units [Marin, Simionescu, &  
309 Barboiu, 2012; Sek, Grucela-Zajac, Krompiec, Janeczek, & Schab-Balcerzak, 2012]. As can  
310 be seen in figure 1a, the imine band in the FTIR spectra of the **C** xerogels is similar in terms  
311 of position and shape, except a left tail of low intensity which belongs to the aldehyde group,  
312 indicating traces of unreacted citral. The intensity of the imine band increased as the citral  
313 content in hydrogels increased, corresponding to a higher density of the imine linkages.  
314 Simultaneously with the appearance of the imine band, the deformation vibration band of the  
315 N-H linkage ( $1556\text{ cm}^{-1}$ ) of the amine units of chitosan drastically diminished in intensity  
316 indicating its consuming. Comparing NMR and FTIR data (Scheme 1) it can be concluded  
317 that the imination reaction further proceeded during the lyophilization process, due to the  
318 slowly removal of water which shifted the reaction equilibrium to the products [Marin et al.,  
319 2014; Marin et al., 2015]. This was possible because of the water H-bonded, residual ethanol  
320 and acetic acid which ensured an appropriate environment for the condensation reaction  
321 [Dinu, Ozmen, Dragan, & Okay, 2007].



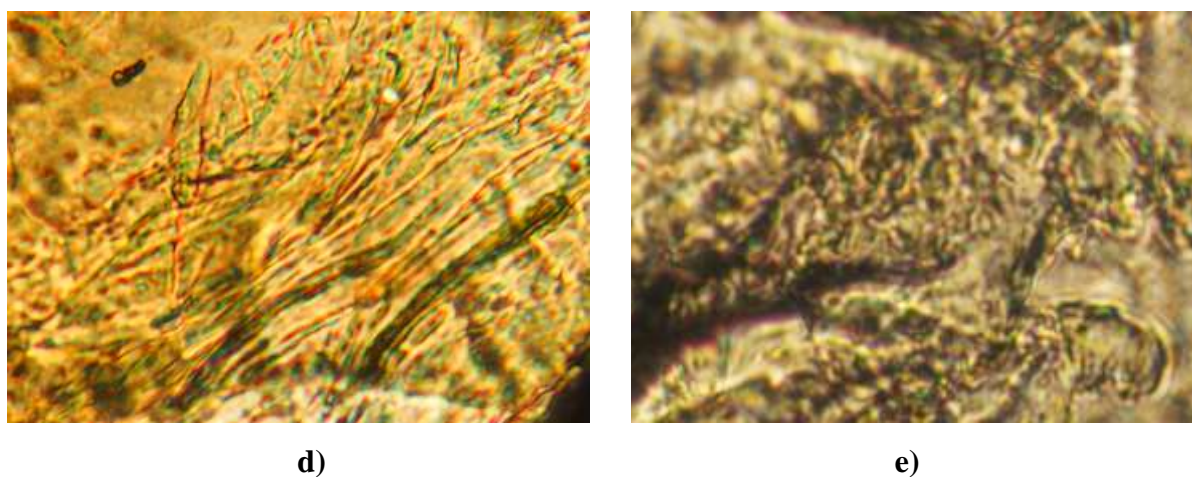
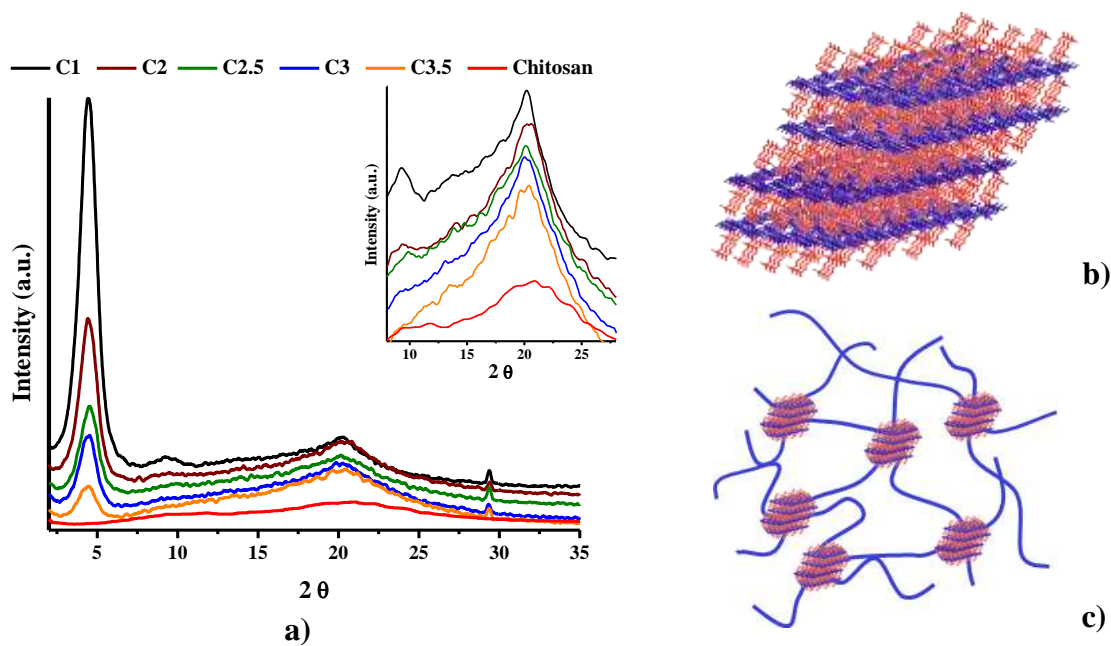
322 **Figure 1.** FTIR spectra of the chitosan, model compound and some representative xerogels

323 The morphology of the solid state of chitosan is dominated by the H-bonds, intra- and  
324 intermolecular ones, reflected in the FTIR spectra in the 2700 – 3700 cm<sup>-1</sup> and 1200 – 1500  
325 cm<sup>-1</sup> domains [Kumirska et al., 2006; Marin et al., 2014]. Thus, in the chitosan spectra  
326 appeared two overlapped bands at 3375 cm<sup>-1</sup> and at 3275 cm<sup>-1</sup> corresponding to the stretching  
327 vibrations of the hydroxyl groups involved in intramolecular and intermolecular H-bonds,  
328 respectively (Figure 1b). In the spectrum of the **MC**, the band corresponding to the  
329 intermolecular H-bonds appeared only as a shoulder, while the band corresponding to the  
330 intramolecular H-bonds was intense, slightly shifted to higher wavenumbers indicating their  
331 prevalence. Looking to the **MC** structure, the formation of an intramolecular H-bond is  
332 favored between the proton of the imine linkage and an oxygen atom of a hydroxyl group of  
333 glucosamine in a neighbor position, giving a more stable six-membered cycle compared to a  
334 five-membered cycle which should be formed by an intramolecular H-bond between the  
335 imine nitrogen and a hydrogen atom of a hydroxyl group of glucosamine. The **C** xerogel  
336 spectra present high similarity in this spectral region with that of the model compound. The  
337 band at 3375 cm<sup>-1</sup> was more shifted to higher wavenumbers as the amount of citral into  
338 xerogels increased, consequence of a close correlation between the formation of the imine  
339 linkages and intramolecular H-bonding. Compared to the model compound, the band at 3275  
340 cm<sup>-1</sup> was still quite intense, indicating the presence of the intermolecular H-bonds, too.

341 Another significant change in the spectra of the MC and xerogels compared to that of  
342 chitosan was revealed in the absorption band characteristic to the CH<sub>2</sub> bending, whose shape  
343 and intensity are strongly correlated to the hydrogen bonds environment. In this region  
344 chitosan exhibited an overlapped band with the intensity maximum at 1405 cm<sup>-1</sup> and a  
345 shoulder at 1377 cm<sup>-1</sup> which underwent significant changes in the case of the xerogel samples,  
346 namely increasing the absorption intensity at 1377 cm<sup>-1</sup>, while decreasing the peak at 1405 cm  
347 <sup>-1</sup> to a shoulder (Figure 1a). This pronounced intensity exchange of the two overlapped bands  
348 indicates considerable alteration of the H-bonds environment given by a drastic modification  
349 of morphology.

### 350 **3.3. Supramolecular characterization**

351 The X-ray diffraction method was involved in order to understand better the influence  
352 of grafting side chain imine units on chitosan on the morphology and therefore on the gelling  
353 process. Chitosan was demonstrated to have a semicrystalline morphology consisting of  
354 ordered clusters of dried chitosan, dispersed into the amorphous state of hydrated chitosan  
355 [Leceta, Guerrero, Ibarburu, Dueñas, & de la Caba, 2013], as evidenced by two broad  
356 overlapped bands with the reflection maxima around 12 and 21 ° (Figure 2a).



357 **Figure 2.** a) WXR curves of chitosan and some representative hydrogels; b) Representation  
 358 of the layered architecture; c) Representation of the hydrogel network for non-stoichiometric  
 359 ratios of the functional groups; d), e) Representative POM microphotographs of **C1** showing  
 360 streaky textures, magnification 200x  
 361

362 Compared to the chitosan X-ray diffractogram, the **C** xerogels have a completely  
 363 different pattern, confirming the drastic morphological changes by imine grafting (Figure 2a).  
 364 Firstly, it was characterized by a very intense reflection band in the small angle domain (4.3 –  
 365 4.7 °) corresponding to a d-spacing of 20.55 – 18.80 Å, defining a layered periodicity. The  
 366 reflection was more intense as the imine linkage density increased, attributed to longer-range  
 367 ordering [Suryanaraya, & Grant, 1998]. In the wide angle domain, the broad reflection band at  
 368 20.4°, caused by the intramolecular distances in chitosan [Leceta, Guerrero, Ibarburu, Dueñas,  
 369 & de la Caba, 2013], was still present, but sharper and of higher intensity attributed to the

370 increasing of the persistence length of the chitosan chains favored by the grafting of the imine  
371 units. The reflection band in the middle angle domain was also sharper and more intense for  
372 xerogels compared to the chitosan, especially in the case of **C1** (characterized by the highest  
373 density of the imine units), attributed to the intermolecular correlations among the imine units  
374 [Ailincai et al., 2016]. As a whole, the X-ray pattern of the studied xerogels is reminiscent of  
375 that of smectic A mesophase of the thermotropic liquid crystals, characterized by a well-  
376 defined periodicity of molecules layers in which the mesogens tend to lay with the long axes  
377 perpendicular to the layer planes and have no long-range positional order of their centers of  
378 mass [Baron, 2001; Dabrowski, 2015; Marin, Destri, Porzio, & Bertini, 2009]. The  
379 explanation of this unusual layering of chitosan obtained by grafting side chain aliphatic units  
380 on its semiflexible backbones can be found if we take in consideration the self-ordering  
381 ability of the imine units stabilized by intramolecular H bonds and the antagonistic nature of  
382 the hydrophilic chitosan and hydrophobic side chain aliphatic imine grafted on it, which  
383 guided the segregation of hydrophilic/hydrophobic layers (Figure 2b). Combining the data of  
384 the three methods of structural characterization (FTIR and NMR spectroscopy and X-ray  
385 diffraction) the scenario of the gelling process can be drawn as follow.

386 At 55 °C, chitosan in solution undergoes the complete destabilization of the intra-  
387 chain H- bonds when the persistence length decreased rapidly and the local stiffness was lost,  
388 chitosan being characterized by a coiled conformation [Rinaudo, 2006]. By adding the citral  
389 solution, the condensation reaction between amino groups of chitosan and aldehyde units of  
390 citral took place *via* imine rigid linkage yielding amphiphilic macromolecules whose  
391 antagonistic building blocks segregated in layers favored by the imine tendency to self-  
392 organize, similar to lyotropic liquid crystals with lamellar mesophases (Figure 2b) [Amar-Iuli,  
393 & Garti, 2006]. Due to the high degree of reversibility of the imine formation in aqueous  
394 medium, the reaction equilibrium between reagents and imine units was reached. Most  
395 probably, the unreacted aldehyde aggregates with the side chain aliphatic tail of the newly  
396 formed imine units grafted on chitosan backbone chain, thus leading to hydrophobic  
397 associations bearing a hierarchical structure with parallel stacked layers (Figure 2b). The  
398 hydrophilic chitosan layers were consolidated by the H-bond system, while those of aliphatic  
399 side chains by hydrophobic interactions, demonstrated as being stronger in the case of  
400 hydrocarbon chains than the aromatic ones [Desbrires, Martinez, & Rinaudo, 1996]. Thus, the  
401 chitosan gelling proceeded once the ordering process took place, being in fact the result of the  
402 competition of three dynamic processes: (i) reversible covalent imine formation (ii) imine  
403 aliphatic side chains self-organization in hydrophobic associations and (iii) segregation of

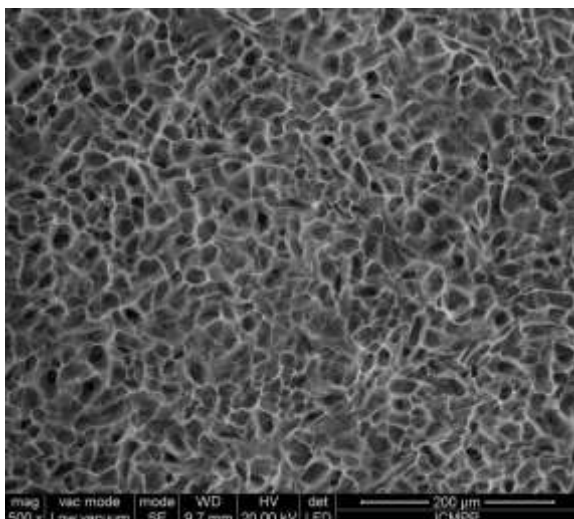
404 hydrophobic/hydrophilic layers. The formation of the hydrophobic layers increased the  
405 accessibility of the unreacted aldehyde to the amine sites and thus favored its conversion into  
406 the imine units by imination and transimination processes which took place under the pressure  
407 of the self-ordering into a hierarchical system of higher stability, specific to the dynamic  
408 imine chemistry [Liu, & Li, 2013]. Moreover, the minimal contact with water of the  
409 hydrophobic layers during the lyophilization process further facilitated the shift of the  
410 reaction equilibrium to the imine products. Taking into account, that (i) no citral loss take  
411 place during lyophilization; (ii) only small traces of citral were evidenced by FTIR; (iii) a  
412 close relationship between the magnitude of long-range layer order and the imine density was  
413 revealed by WXR, it can be considered that a lamellar structure was reached in the case of  
414 **C1** (Figure 2b), and ordered lamellar entities acting as multibinder net nodes of chitosan free  
415 chains in the case of the other hydrogels (Figure 2c). As the reaction took place in non-  
416 equimolar conditions, the size and density of the lamellar entities varied with the imine  
417 linkage density. The formation of the supramolecular net nodes has been also suggested by  
418 TEM measurements, when black spots could be distinguished (Figure S4).

419 A supramolecular arrangement has to show a distinct texture when viewed through a  
420 cross-polarized microscope [Baron, 2001; Dabrowski, 2015; Marin, Destri, Porzio, & Bertini,  
421 2009]. As can be seen in figure 2d,e, the hydrogels exhibited “streaky” birefringent textures  
422 under polarized light, typical to lamellar mesophases of the lyotropic liquid crystals, once  
423 more confirming the supramolecular architecture of the hydrogels.

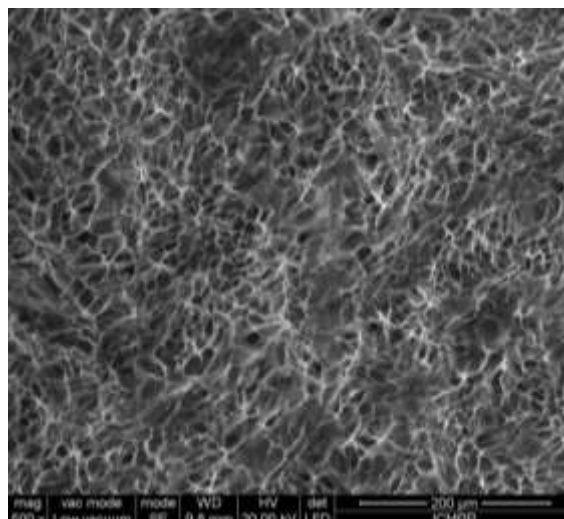
424

### 425 **3.4. Hydrogel microstructure**

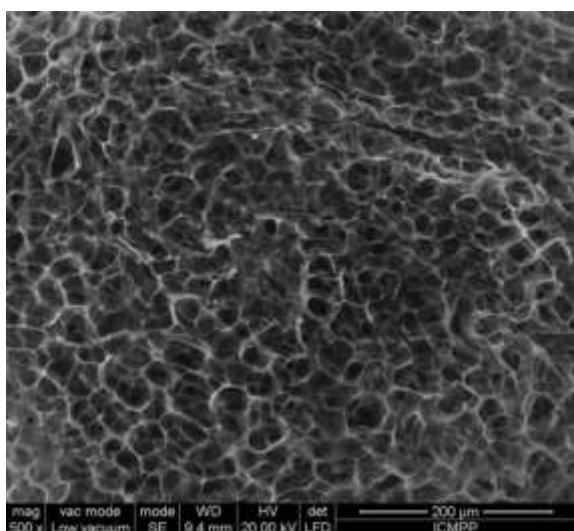
426 The xerogels showed a sponge-like microstructure with pore diameter varying with the  
427 content of aldehyde crosslinker in each hydrogel; the pore diameter increased from 14 to 26  
428  $\mu\text{m}$  as the content of citral decreased (Figure 3). The hydrogels with smaller amount of citral  
429 and so lower density of lamellar entities and higher density of hydrophilic chitosan showed  
430 larger pores. Compared to other chitosan hydrogels [Marin et al., 2014], they had smaller  
431 inner pore size, attributed to the hydrophobic citral layers which limited the water entrapping  
432 during the gelling process.



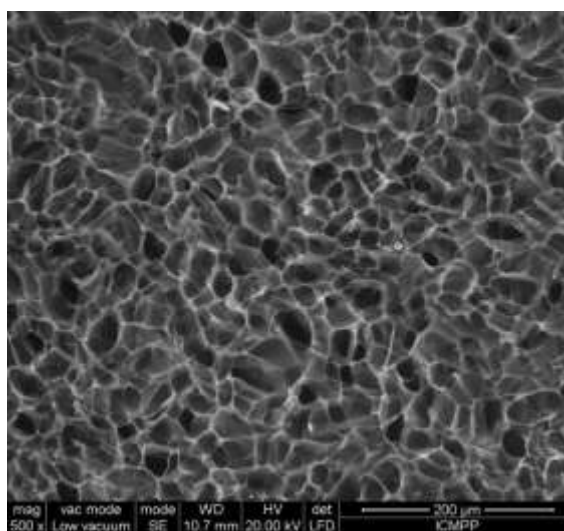
**C1**



**C2**



**C2.5**



**C3.5**

**Figure 3.** SEM microphotographs of the hydrogels

433

434

### 435 **3.5. Rheological properties**

436 Rheological investigations of the studied hydrogels were performed in order to gain  
 437 information related to their mechanical strength correlated to their crosslinking degree and  
 438 subsequent to their supramolecular architecture. In frequency sweep experiments, carried out  
 439 at 20 °C in the linear domain of viscoelasticity, the samples showed the dominance of the  
 440 elastic component over the viscous one ( $G' > G''$ , solid-like behavior) for molar ratios of  
 441  $\text{NH}_2/\text{CHO}$  below 3.5 (**C1-C3.5**). The values of the elastic modulus are high at high  
 442 frequencies, comparable with those of hydrogels obtained using multi-branched crosslinkers  
 443 [Wang et al., 2010], indicating robust mechanical properties. Particularly, the value of the  
 444 elastic modulus of the **C1** hydrogel with layered morphology is significant higher compared



445 to the other hydrogels cross-linked by supramolecular entities (from 5 to 72 times, as the  
 446 crosslinking degree decreased) (Table S1). As the NH<sub>2</sub>/CHO molar ratio increased, the  
 447 viscous component became slightly dominant over the elastic one ( $G' < G''$ ) in the case of the  
 448 C4.5 sample, indicating a liquid-like behavior near the gel point (Figure 4a). Considering the  
 449 power law dependence of the viscoelastic moduli on frequency,  $G'(\omega) \sim \omega^{n'}$  and  $G''(\omega) \sim$   
 450  $\omega^{n''}$ , the gel point was determined, according to Chambon and Winter [Chambon, & Winter,  
 451 1987], which established that at the gel point,  $n' = n'' = n$ , and the following scaling law is  
 452 valid:

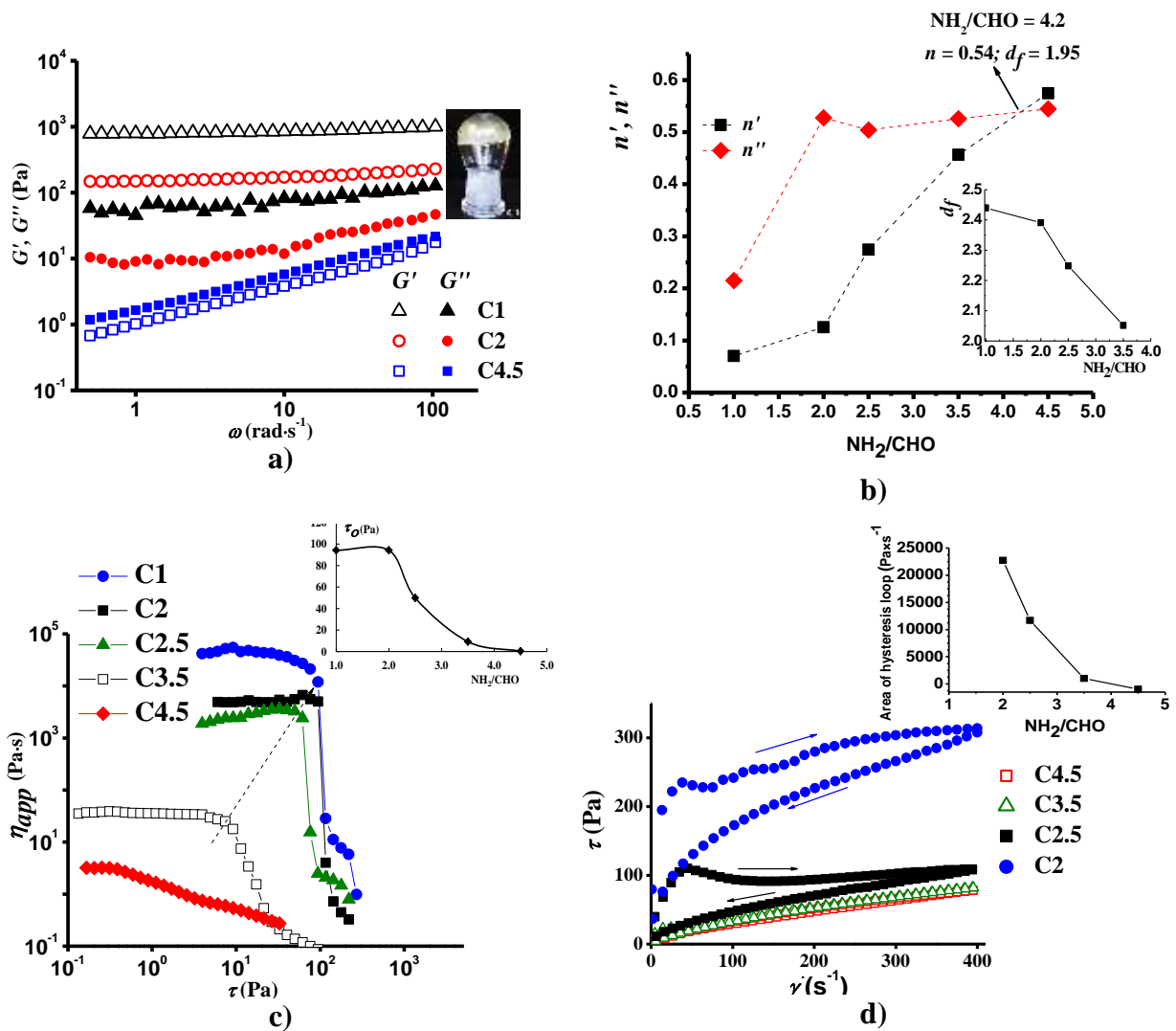
$$G'(\omega) = G''(\omega) \sim \omega^n \quad 0 < n < 1 \quad (1)$$

453 where  $n$  is the relaxation exponent which can give the indication about the material structure.  
 454 As can be seen from the representation of the variation of the exponents  $n'$  and  $n''$  (obtained  
 455 by fitting the frequency dependence data of  $G'$  and  $G''$  in the frequency range of 10-100 rad·s<sup>-1</sup>)  
 456 with the crosslinker content, the NH<sub>2</sub>/CHO ratio corresponding to the sol-gel transition was  
 457 established at about 4.2 ( $n = 0.54$ ) (Figure 4b).

458 The relaxation exponent,  $n$ , allows the determination of the fractal dimension,  $d_f$ , a  
 459 parameter in a three-dimension space, using the relation proposed by Muthukumar  
 460 [Muthukumar, 1989].

$$d_f = (10n - 15) / (2n - 6) \quad (2)$$

461 The value of the fractal dimension (calculated with  $n'$ ) progressively increased from 2.05  
 462 (C3.5) to 2.44 (C1), as the citral content increased (the inset in Figure 4b, Table S1), with a  $d_f$   
 463 value of 1.95 at the gel point (NH<sub>2</sub>/CHO = 4.2). Generally, the values of  $d_f$  are comprised  
 464 between 1 and 3, the higher ones corresponding to a more compact network structure  
 465 [Chambon, & Winter, 1987]. In this light, the variation of the  $d_f$  agrees well with the degree of  
 466 crosslinking of the hydrogels, indicating a denser structure for the lamellar architecture (C1)  
 467 in comparison to chitosan cross-linked by supramolecular entities (C2-C3.5).



468 **Figure 4.** a) Viscoelastic moduli,  $G'$  and  $G''$  as a function of the oscillation frequency,  $\omega$ , at  
 469 20 °C, for representative hydrogels; b) variation of  $n'$ ,  $n''$  exponents (at 20 °C, in the  
 470 frequency range of 10-100 rad·s<sup>-1</sup>) as a function of  $\text{NH}_2/\text{CHO}$  ratio (the inset figure represents  
 471 the dependence of the fractal dimension on  $\text{NH}_2/\text{CHO}$  ratio); c) variation of  $\eta_{app}$  as a function  
 472 of  $\tau$  for all investigated samples at 20 °C (the inset figure represents dependence of  $\tau_0$  on the  
 473  $\text{NH}_2/\text{CHO}$  ratio); d) flow curves of representative hydrogels at 20 °C (the inset figure  
 474 represents variation of hysteresis loop area with  $\text{NH}_2/\text{CHO}$  ratio)

475

476 Other parameters which bring information related to the viscoelastic properties of the  
 477 hydrogels are the yield stress ( $\tau_0$ ) and zero shear viscosity ( $\eta_0$ ). The yield stress of the samples  
 478 was determined as the value at which the apparent viscosity ( $\eta_{app}$ ) abruptly decreased as a  
 479 function of shear stress (as shear stress ( $\tau$ ) was progressively increased) (Figure 4c).

480 The **C1-C3.5** hydrogel samples have shown a pseudoplastic behavior (shear-thinning  
481 behavior) with yield stress, while the **C4.5** sample did not reveal any yield stress. The  
482 hydrogels prepared with high amounts of citral (**C1, C2**) have shown the highest  $\tau_o$  values  
483 (around 90 Pa) pointing to the formation of stiff and strong networks (in agreement with the  
484 X-ray measurements), while those with low citral content (**C3.5**) displayed a significant  
485 decline of  $\tau_o$  to 9 Pa (of about tenfold) indicating a softer hydrogel with easier spreadability  
486 (inset of the Figure 4c).

487 Zero shear viscosity ( $\eta_o$ ) values of the samples **C1-C4.5** as determined by applying  
488 the simplified Carreau equation to data from flow curve (the dependence of  $\eta_{app}$  on the shear  
489 rate ( $\dot{\gamma}$ )) (Table **S1**) [Carreau, 1972] also drastically increased as the content of citral  
490 increased, from 3.5 Pa·s for **C4.5** sample to 46 880 Pa·s for **C1** sample. The drastic increment  
491 of four orders of magnitude of the  $\eta_o$  is in agreement with the longer range layering (see X-  
492 ray data), revealing a close correlation between the supramolecular architecture and the  
493 hydrogel stability under the continuous shear stress of the hydrogels. Specifically, zero shear  
494 viscosity ( $\eta_o$ ) of the **C1** hydrogel with layered architecture is about one-two orders of  
495 magnitude higher compared to the other hydrogels cross-linked by supramolecular entities  
496 (Table **S1**).

497 The oscillatory shear measurements at two different temperatures: 20 °C and 37 °C,  
498 evidenced a clear effect of the temperature on the viscoelastic parameters, especially in the  
499 case of the hydrogels crosslinked with a small quantity of citral. The elastic modulus ( $G'$ ) and  
500 the complex viscosity ( $\eta^*$ ) of the investigated samples increased with the temperature (except  
501 **C2**) (Table **S1**). The **C2.5** and **C3.5** hydrogels undergo significant increasing of  $\eta^*$  at 37 °C  
502 indicating a stronger hydrogel network at the body temperature (Figure **S5**). This behavior is  
503 in agreement with the shift of the reaction equilibrium to the imine at higher temperature  
504 [Tang et al., 2007] and subsequent intensification of the hydrophobic interactions.

505 Thixotropic behavior of the samples was investigated by following the hysteresis loop  
506 formed by the flow curve at the increasing the shear rate up to 400 s<sup>-1</sup> followed by its  
507 decreasing (Figure 4d). The magnitude of the hysteresis loop gives the indication on the  
508 degree of time dependency and the hysteresis area represents the energy *per* time and volume  
509 consumed in the structure breakdown. The hysteresis area is accepted to be positive for the  
510 systems with thixotropic behavior and negative if the behavior is rheopexic.

511 The hydrogels exhibited the upward curve above the downward curve - indicating a  
512 thixotropic behavior, while the liquid like sample **C4.5** showed the upward curve below the

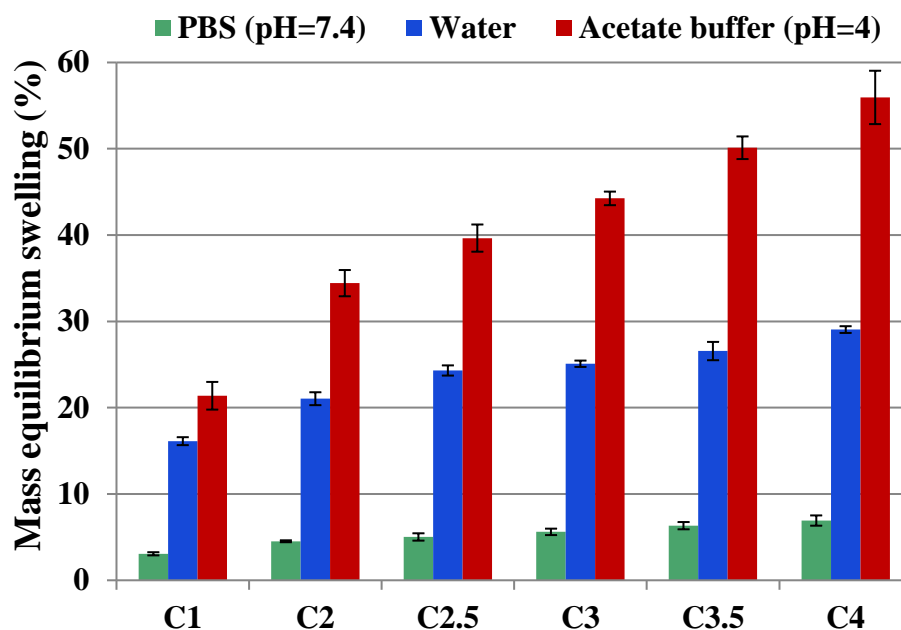
513 downward curve – indicating a rheotropic behavior (Figure 4d). The upward curves of **C2** and  
514 **C2.5** samples present a stress overshoot (with a maximum value at about  $40\text{ s}^{-1}$ ) which can be  
515 explained by the necessity of applying a higher stress to break their strong structure and to  
516 start the flow. The sample **C3.5** with smaller content of citral showed a low area of hysteresis  
517 loop indicating that lower stress is necessary to break its weak structure. Thereby, **C2** and  
518 **C2.5** hydrogels show a strong thixotropy and **C3.5** a weak one.

519 The inset of figure 4d presents the dependence of the area of hysteresis loop on the  
520 crosslinker content. The hysteresis areas for **C2** and **C2.5** samples were  $22\,740\text{ Pa}\cdot\text{s}^{-1}$  and  $11\,690\text{ Pa}\cdot\text{s}^{-1}$ ,  
521 respectively, corresponding to stable structures that requires a higher energy for  
522 the structural regeneration. The investigated samples (except **C4.5**) showed a beginning of the  
523 hysteresis cycle higher than the final of the cycle, meaning that the initial apparent viscosity is  
524 higher than the final one. The percentage of the regeneration of viscosity ( $\eta_{reg}$ ), calculated  
525 considering the viscosity value at the end of the test and the initial viscosity as reference, was  
526 found to be about 20% for **C2-C3.5** samples (Table S1).

### 527 **3.6. Swelling behavior**

528 Swelling behavior of the hydrogel samples was investigated in phosphate buffer  
529 solution (PBS) with a pH of 7.4, close to that of biological tissues and acetate buffer solution  
530 with a pH of 4, close to the one of stomach. Water was used for water uptake calculation. The  
531 mass equilibrium swelling (MES) was reached in three hours in acetate buffer, while in water  
532 and PBS it was slower, attaining the MES in 24 hours. For all the 3 media of different pH, the  
533 MES increased as the content of citral and consequently of hydrophobic associations  
534 decreased almost three fold in the case of acetate buffer solution (Figure 5). Remarkably, the  
535 xerogel samples had the MES values of about 5 times lower in PBS compared to neutral  
536 water, mostly attributed to the greater stability of the imine units in a basic solution, which  
537 suggested better preservation of the supramolecular architecture of the hydrogels in tissue  
538 engineering applications. On the contrary, the MES values were about 2 times higher in  
539 acetate buffer compared to neutral water, because of the faster reversibility of the imine bond  
540 in acidic solution resulting in the diminishing of the crosslinking density. The xerogel samples  
541 dissolved completely in 5 days in acetate buffer, while in water and phosphate buffer  
542 remained unaffected over a month. There was a close correlation between the crosslinking  
543 degree of the hydrogels and their swelling ability; the hydrogels with lower crosslinking  
544 degree and thus high amount of free hydrophilic chitosan swelled about 3 times more  
545 compared to the hydrogels with higher crosslinking degree.

546 The measurements were performed in triplicate and no significant differences were  
547 observed between the three samples.



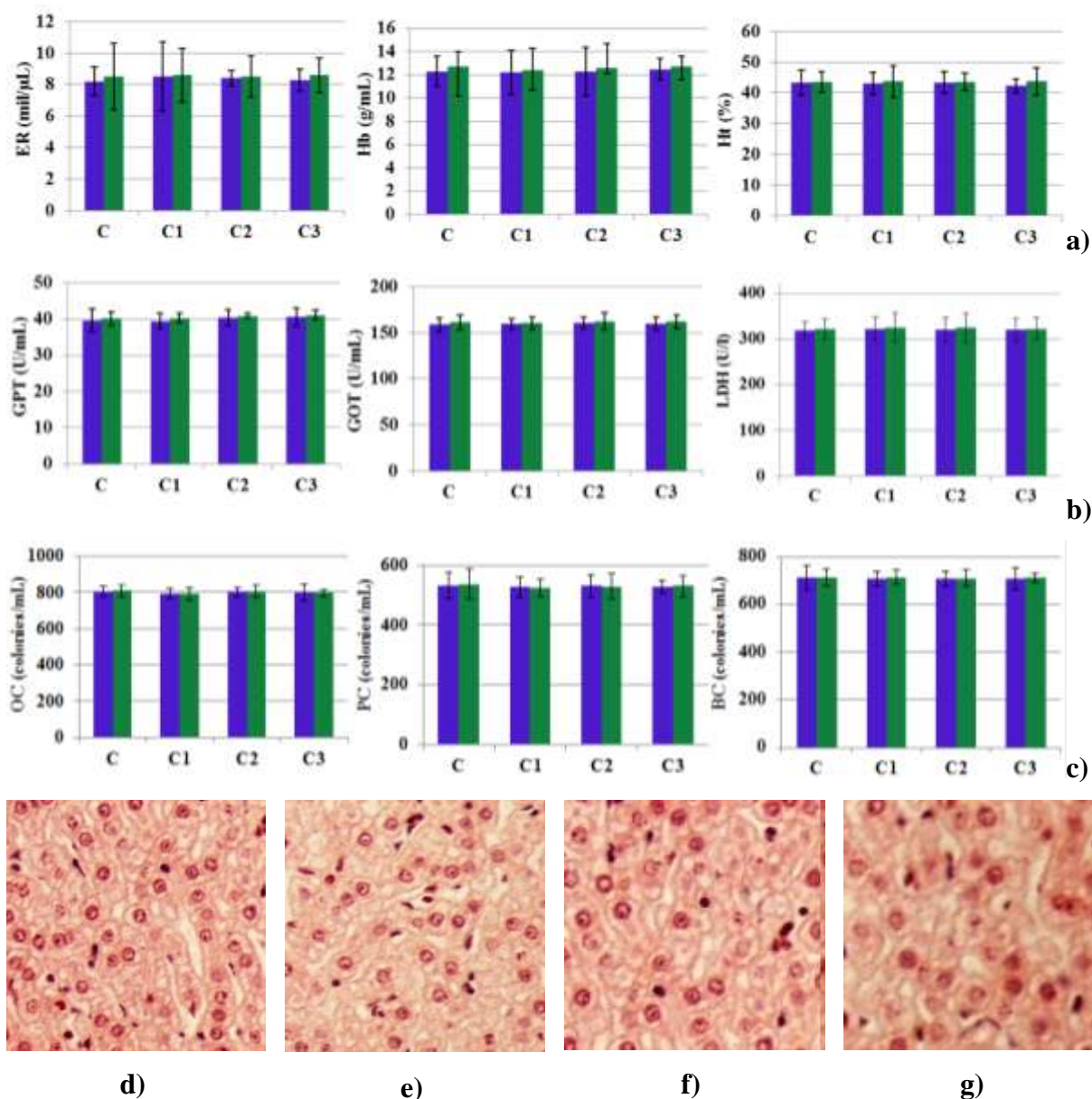
548  
549 **Figure 5.** Mass equilibrium swelling of the hydrogels  
550

### 551 **3.7. Evaluation of the *in vivo* biocompatibility of the hydrogels**

552 In order to use the synthesized hydrogels in bio-applications, their impact on the living  
553 organisms has been studied *in vivo* on mice, by intraperitoneal administration and  
554 determination of the hematological, biochemical and immune system profile.

555 The haematological tests revealed no significant changes in the number of  
556 erythrocytes, in the hemoglobin and hematocrit values, between the animals treated with **C1**,  
557 **C2**, and **C3** hydrogels compared to the animals from the control group (**C**), after 24 hours  
558 and, also, after 14 days of the experiment (Figure 6a). The values of the leukocyte formula  
559 elements - polymorphonuclear neutrophils, lymphocytes, eosinophils, monocytes, basophils -  
560 in the blood collected from the animals that received **C1**, **C2**, and **C3** respectively, were at  
561 comparable levels to those of saline-treated animals (Table S2). The hematological  
562 parameters in the normal range show the absence of a systemic inflammatory reaction related  
563 to the lack of toxicity of the hydrogels.

564



565 **Figure 6.** a) The levels of blood erythrocytes, hemoglobin and hematocrit in animals  
 566 treated with **C1**, **C2**, and **C3** after one day (■) and after 14 days (■); b) The levels of GPT,  
 567 GOT and LDH in animals treated with **C1**, **C2**, and **C3** and control group (**C**) after one day (■)  
 568 and after 14 days (■); c) The levels of OC, PC and BC in animals treated with **C1**, **C2**,  
 569 and **C3** after one day (■) and after 14 days (■); The optical microscopy analysis of the liver  
 570 tissue samples of d) **Control** group; e) **C1**; f) **C2**; g) **C3**; – section of liver. H&E stain x10.

571  
 572 Changes in the level of the alanine aminotransferase (GPT), the aspartate  
 573 aminotransferase (GOT) and the lactic dehydrogenase (LDH) are commonly used as  
 574 biochemical markers for liver function. As can be seen in figure 6b no statistically significant  
 575 variations in the levels of GPT, GOT and LDH were noticed in the animals treated with **C1**,

576 **C2**, and **C3** hydrogels compared with the control animals, indicating a normal liver function  
577 with no observable toxicity of the studied hydrogels. Moreover, the histopathological  
578 examination of the samples prepared from liver tissue fragments of the control group animals  
579 (Figure 6d) and from animals treated with **C1**, **C2**, and **C3** respectively (Figure 6e,f,g), did  
580 not reveal any obvious changes of the normal liver architecture.

581 The results of immunological tests are illustrated in figure 6c. Again, as can be clearly  
582 seen from the graphs, the levels of the determined immune parameters (serum opsonic,  
583 phagocytic and bactericidal capacities) corresponding to the animals treated with **C1**, **C2**, and  
584 **C3** hydrogels, almost match the values of the control and are strongly supported by similar  
585 statistically insignificant variations. This means that the understudy hydrogels are not  
586 perceived by the immune system as dangerous or even non-self and consequently they do not  
587 stimulate an immune response in the body.

588 In conclusion, the synthesized citral-chitosan hydrogels did not induced any  
589 significant haematological, biochemical, immunological and histological modifications in the  
590 laboratory animals, proving *in vivo* biocompatibility under the experimental conditions.

591

## 592 **CONCLUSIONS**

593 Hydrogels based on chitosan and citral – two reagents from natural sources, were  
594 successfully prepared and characterized. Following the results of structural analysis, the  
595 driving force which guided the unprecedented gelling of chitosan with citral monoaldehyde  
596 was established to consist in the forming of glycodynamers by grafting dynamic imine units  
597 onto the static chitosan backbones assisted by their self-ordering through supramolecular  
598 interactions in layered architectures with role of chitosan multibinders. The ordering process  
599 was favored by the reversible nature of the imine linkages, by imination and transimination  
600 reactions which took place under the pressure of reaching a hierarchical structure of higher  
601 stability. The resulted network consisting in chitosan chains linked by the newly formed  
602 multibinders, determines robust mechanical properties, comparable with those obtained when  
603 using multi-branched crosslinkers or those appropriate to hydrogels with layered morphology  
604 given by using metallic nanosheets. The gelling process took place for low amounts of citral,  
605 starting to a 4.2/1 molar ratio of amino/aldehyde functional groups. The hydrogels were  
606 highly elastic and they showed thermo-responsiveness and thixotropic behavior. They had a  
607 sponge-like microstructure and swelled well in water and acidic solution but retained their  
608 shape in PBS solution at tissue pH. Their morphology could be tuned by the crosslinking  
609 degree.

610 As expected, the evaluation of the *in vivo* biocompatibility of the hydrogels, monitored  
611 on laboratory mice, did not result in any abnormal changes in the hematological, biochemical  
612 and immune system profile, recommending their safe use in bio-applications.

613 The paper brings into attention a novel hydrogel with real chances for bio-  
614 applications. Moreover, it illustrates a novel method of crosslinking chitosan using  
615 monoaldehydes which are abundant in nature and have own valuable therapeutic properties.

616

## 617 **ACKNOWLEDGEMENTS**

618 The research leading to these results has received funding from the Romanian  
619 National Authority for Scientific Research, MEN – UEFISCDI grant, project number PN-II-  
620 RU-TE-2014-4-2314. This publication is part of a project that has received funding from the  
621 European Union's Horizon 2020 research and innovation programme under grant agreement  
622 667387.

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